

(12)

EUROPEAN PATENT APPLICATION

(21) Application number: 86304215.6

(51) Int. Cl.⁴: G 10 K 11/02

(22) Date of filing: 03.06.86

(30) Priority: 04.06.85 GB 8514052

(43) Date of publication of application:
25.02.87 Bulletin 87/9

(84) Designated Contracting States:
AT BE CH DE FR GB IT LI LU NL SE

(71) Applicant: Ed. Geistlich Söhne A.G. für Chemische
Industrie

CH-6110 Wolhusen Lucerne(CH)

(72) Inventor: Wokalek, Heinrich Albert-Ludwig-Universitaet
Freiburg, Hautklinik Hauptstrasse 7
D-7800 Freiburg 1 Br.(DE)

(72) Inventor: Strasser, Wolfgang
Albert-Ludwig-Universitaet
Freiburg, Hautklinik Hauptstrasse 7
D-7800 Freiburg 1 Br.(DE)

(74) Representative: Holmes, Michael John et al,
Frank B. Dehn & Co. Imperial House 15-19 Kingsway
London WC2B 6UZ(GB)

(54) **Acoustic coupling medium for transmitting ultrasound.**

(57) An acousting coupling medium for transmitting ultrasound is disclosed. The medium, which is of use in ultrasonic visualisation of the human body, comprises a sheet of hydrogel containing over 90% water.

EP 0 211 482 A2

JD 50 656

"Compositions"

This invention concerns improvements in or relating to coupling media for transmitting ultrasound, in particular for ultrasonic diagnosis.

Ultrasonic diagnosis represents an extremely
5 safe and well-tolerated technique for investigation
of the human body and, indeed, for investigation
of other structures. It is of especial use in
relation to young children or neonates where X-
ray visualisation is inadvisable, particularly
10 in screening programs. Other valuable areas of
use include cerebral and cardiological visualisation
and visualisation of superficial body structures
such as the breast.

The available ultrasonic visualisation devices
15 are, in use, directly applied to the area of the
body to be studied and it is essential that the
device makes virtually perfect contact with the
appropriate body surface. Conventionally, ointment-
like gels have been applied to the body surface
20 as coupling media to ensure such contact. However,
materials of this type must be used with care to
ensure that there are no air bubbles between the
acoustic device and the body surface. They may
be impracticable or unsuitable for application
25 in some cases, for example where the body surface
is cut or abraded or body organs exposed during
surgery are to be visualised and are frequently
found to transmit sound inefficiently.

More recently, coupling media in the form
30 of plastic bags containing thickened aqueous solutions
have been proposed but these have been relatively
expensive and have not always proved effective,
in particular absorbing a large amount of sonic
energy.

We have now found that hydrogels in sheet form provide extremely effective acoustic coupling media for transmitting ultrasound; especially good results are obtained if the gels contain over 90%, preferably over 95%, by weight of water, since their acoustic properties then approximate closely to those of the soft tissues of the body.

According to the present invention therefore we provide an acoustic coupling medium for transmitting ultrasound comprising a sheet of a hydrogel material containing over 90% by weight of water.

According to a further aspect of the invention we provide a process for the preparation of an acoustic coupling medium for transmission of ultrasound whereby a hydrogel containing over 90% by weight of water is prepared in sheet form.

Hydrogel sheets may readily be formed from hot aqueous solutions of gel-forming natural or synthetic polymers, for example polysaccharides such as agar, carrageenin, alginates and pectins (especially low methoxy pectins) and polypeptides and proteins such as gelatin. Alternatively, hydrogel sheets may be formed by polymerisation of water-soluble vinyl monomers in aqueous solution in the presence of a cross-linking agent such as a polyfunctional vinyl compound. Examples of such monomers include acrylic and methacrylic acid and their salts, amides and N-substituted amides, N-vinyl pyrrolidone and vinyl ethers of C₁₋₅ alkanols. Examples of cross-linking agents include ethylene glycol bis-acrylate, N,N'-methylene-bis-acrylamide, divinyl ether and diallyl maleate. It is also possible to produce hydrogel sheets by cross-linking water soluble polymers using cross-linking agents or ionising radiation followed by re-swelling with water; thus, for example, a film of polyvinyl alcohol may be cross-linked with ethylene diisocyanate

while a sheet of high molecular weight polyethylene glycol may be cross-linked by irradiation with Co^{60} gamma rays.

A still further possibility is to prepare
5 cross-linked gelatin sheets by cross-linking aqueous gelatin with an aldehyde such as formaldehyde or glyoxal or by addition of a polyvalent metal salt such as aluminium sulphate.

Particularly good results have been obtained
10 using hydrogels which contain a gel-forming protein, polypeptide or polysaccharide (such as one of those mentioned above) the chains of which are interspersed with chains of a hydrophilic synthetic polymer (such as one of the vinyl polymers mentioned above). Particularly
15 useful gel-forming proteins and polysaccharides include gelatin and agar. The synthetic polymer is preferably an acrylic polymer having hydrophilic groupings, polyacrylamide being especially useful. The cross-linking agent is preferably an acrylate compound
20 having at least two double bonds, for example N,N'-methylene-bis-acrylamide.

Such gels are capable of retaining large amounts of water while having excellent mechanical strength and good surface properties such as smoothness and
25 lack of tackiness.

The hydrogel may conveniently contain 2 to 10% of the protein, polypeptide or polysaccharide and hydrophilic polymer together with the hydrophylic synthetic polymer, preferably containing 1 to 5%
30 of the protein, polypeptide or polysaccharide and 1 to 5% of the synthetic polymer.

In order to ensure the sterility of the hydrogel, it may advantageously contain a disinfectant, conveniently an antibacterial compound such as taurolidine. The
35 hydrogels thus may be kept in the fully hydrated state, for example in a water bath, for several months without microbial contamination.

The hydrogel is preferably used in the form of uniform, parallel-sided sheets. The thickness of the sheets is preferably in the range 3 to 25 mm e.g. 4 to 15 mm. In general, the sheets may be
5 of a shape corresponding to the acoustic device, for example discs. The optimum thickness may depend on the position of the body structure to be visualised, that is the required focus of the ultrasonic device.

As indicated above, the hydrogels according
10 to the invention exhibit excellent acoustic properties in transmitting sound in the frequencies commonly used in ultrasonic diagnosis, that is 5-10 MHz.

Thus, the sheet material of the invention may be used in conjunction with a scanning ultrasound
15 diagnostic device with a 5 or 7.5 MHz transducer (a so-called B-scan device).

In the examination of superficial structures of the body, such as the thyroid gland or the breast, the hydrogel provides an efficient coupling medium
20 which also, by spacing the head of the ultrasonic device from the structure in question, brings the latter into the optimal zone of examination of the device. There is excellent contact between the skin and the hydrogel and between the hydrogel and the
25 ultrasonic device, with no air spaces or other voids which could affect acoustic transmission.

The hydrogel may be used advantageously in postoperative or intraoperative ultrasonic examinations as well as preoperative and screening examinations
30 and may be directly applied not only to the skin but also to organs of the body exposed by surgery. As indicated, the use of the hydrogel as coupling medium may serve to bring the structure under examination into optimum focus.

35 The hydrogels here concerned may be prepared by forming the hydrophilic synthetic polymer in an aqueous solution containing the gel-forming protein,

polypeptide or polysaccharide. Thus, a preferred hydrogel according to the invention may be prepared by dissolving acrylamide and an appropriate cross-linking agent such as N,N'-methylene-bis-acrylamide in an aqueous dispersion of agar and effecting polymerisation. When polymerisation is complete, any excess reagents can be removed by thorough washing, an antibacterial substance optionally being introduced at this stage. If desired, the gel may be partially dried for convenience in handling and storage and rehydrated prior to use.

The following Example is given by way of illustration only:

15 Example:

20g of agar-agar are suspended under agitation in 880g of deionized water and heated to 95°C until complete dissolution. 1 l of a second aqueous solution containing 70g of acrylamide and 1.84 g of N,N'-methylene-bis-acrylamide is prepared at ambient temperature and added to the first solution with thorough mixing. Under continued agitation, 2.2 g of N,N,N',N'-tetrakis-(2-hydroxypropyl)-ethylene diamine dissolved in 60 g of water and then 1.26 g of ammonium peroxodisulfate dissolved in 40 g of water are added. The solution is poured into moulds to provide, after polymerization, 100mm x 200mm sheets of thickness 10mm containing over 95% by weight of water.

The mixture has a temperature between 50°C and 55°C and begins to polymerize immediately. After 10 minutes the gel point is reached. The batch is allowed to cool down overnight during which time polymerization is completed.

The gel is freed from soluble impurities by washing in pure flowing water for 24 hours.

Sheets of acoustic coupling medium as prepared above have been used in dermatological sonographic studies, including diagnosis of lymph node metastases, congenital nevis, malignant melamona and granuloma
5 pyogenicum, using a B-scan ultrasonic device.

CLAIMS:

1. An acoustic coupling medium for transmitting ultrasound comprising a sheet of a hydrogel material containing over 90% by weight of water.
- 5 2. A coupling medium as claimed in claim 1 containing over 95% by weight of water.
3. A coupling medium as claimed in claim 1 or claim 2 in which the hydrogel contains a gel-forming protein, polypeptide or polysaccharide the chains
10 of which are interspersed with chains of a hydrophilic synthetic polymer.
4. A coupling medium as claimed in claim 3 in which the hydrogel comprises agar as a gel forming poly-saccharide and polyacrylamide as the hydrophilic
15 synthetic polymer.
5. A coupling medium as claimed in any of the preceding claims in which the hydrogel is in the form of uniform, parallel-sided sheets the thickness of which is in the range 3 to 25 mm.
- 20 6. The use of a sheet of hydrogel material containing over 90% by weight of water as an acoustic coupling medium for transmitting ultrasound.
7. The use as claimed in claim 6 wherein said coupling medium is used in ultrasound diagnosis.
- 25 8. A process for the preparation of an acoustic coupling medium for transmission of ultrasound whereby a hydrogel containing over 90% by weight of water is prepared in sheet form.

9. A process as claimed in claim 8 in which a hydrophilic synthetic polymer is formed by polymerisation in an aqueous solution containing a gel-forming protein, polypeptide or polysaccharide.
- 5 10. A method for transmitting ultrasound in which an acoustic coupling medium is used which comprises a sheet of hydrogel material containing over 90% by weight of water.